1088 Technical Briefs

HDL particle aggregates after precipitation of apo B-containing lipoproteins.

The data on HDL particle size obtained in this study (mean diameter, 8.8 nm) are in agreement with the values described in the literature for other techniques. In healthy normolipidemic individuals, HDL sizing by nuclear magnetic resonance spectroscopy yielded diameters of ~9.2 nm (10), whereas the values obtained from gradient gel electrophoresis ranged from 8.4 to 9.6 nm (9, 13). In this study, similar to other published results obtained by gradient gel electrophoresis (13), the HDL particle diameter (nm) was greater in premenopausal women than in men (9.1 vs 8.4 nm; Mann-Whitney test, P = 0.013). Negative correlations between HDL particle size and total cholesterol and LDL-cholesterol were also reported by Pascot et al. (13), thus strengthening the link between HDL particle size and coronary artery disease. In the present study, the correlations between HDL particle size and HDL-cholesterol and triglyceride concentrations were not statistically significant, probably because of the small number of samples. Pascot et al. (13) may have found significant correlations for these relationships because they studied >400 individuals. Therefore, LLS analysis after chemical precipitation of apo B-containing lipoproteins gave results for HDL diameter in the same range as those obtained by established techniques for lipoprotein sizing (9, 10, 13). Furthermore, the differences between genders and the correlations reported here are in agreement with those described in the literature (13).

Because LLS analysis after chemical precipitation is a practical and less time-consuming approach for HDL sizing, it could be used in large trials and in routine clinical laboratory analysis.

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Quantitative Assessment of PML-RARa and BCR-ABL by Two Real-Time PCR Instruments: Multiinstitutional Laboratory Trial, Pascual Bolufer,1* Dolors Colomer,2 Maria T. Gomez,³ Joaquín Martínez,⁴ Silvia M. Gonzalez,³ Marcos Gonzalez,⁵ Josep Nomdedeu,⁶ Beatriz Bellosillo,⁷ Eva Barragán,¹ Francesco Lo-Coco,⁸ Daniela Diverio,⁹ Lourdes Hermosin, ¹⁰ José García-Marco, ¹¹ Maria D. de Juan, ¹² Francisco Barros, ¹³ Rafael Romero, ¹⁴ and Miguel A. Sanz, ¹⁵ for the Group of Molecular Biology in Hematology (1 Molecular Biology, Department of Medical Biopathology, Hospital Universitario La Fe, Avda Campanar 21, 46009 Valencia, Spain; ² Hematopathology Unit, Hospital Clínic, Barcelona, Spain; ³ Molecular Biology, Hematology, Hospital Gran Canaria Dr. Negrin, Las Paslmas de GC, Spain; 4 Molecular Biology, Hematology, Hospital 12 de Octubre, Madrid, Spain; ⁵ Immunopathology and Molecular Biology, Hematology, Hospital Clínico Universitario, Salamanca, Spain; ⁶ Laboratory of Hematology, Hospital de la Santa Creu i Sant Pau, Barcelona, Spain; ⁷ Laboratory of Cytogenetics and Molecular Biology, Service of Pathology, Hospital del Mar, Barcelona, Spain; 8 Laboratory of Integrated Diagnosis of Oncohematologic Diseases, University Tor-Vergata, Rome, Italy; ⁹ Laboratorio di Diagnostica Molecolare Oncoematologica, Dipartimento di Biotecnologie Cellulari ed Ematologia, Universitá degli Studi "La Sapienza", Rome, Italy; 10 Biology, Hematology, Hospital de Jerez, Jerez de la Frontera, Cádiz, Spain; 11 Molecular Cytogenetic Unit, Servicio de Hematologia, Hospital Universitario Puerta de Hierro, Madrid, Spain; ¹² Unified Laboratory, Immunology, Hospital Donostia, San Sebastian, Gupuzcoa, Spain; ¹³ Molecular Medicine Unit-INGO (Sergas), University of Santiago de Compostela, Hospital Clínico Universitario de Santiago, Santiago de Compostela, Spain; ¹⁴ Departamento de Estadistica e Investigación Operativa, Universidad Politécnica de Valencia, Valencia, Spain; 15 Clinical Hematology, Service of Hematology, Hospital Universitario La Fe, Hospital Universitario La Fe, Valencia, Spain; * author for correspondence: fax 34961973030, e-mail bolufer_pas@gva.es)

The recent introduction on the market of instruments for real-time PCR has prompted the development of quanti-

Table 1. Results of the *PML-RARa* and *BCR-ABL* assays (copies/ μ L) for the participating laboratories grouped according to the instrument.

Laboratories LC ABI Assay Samples BCR-ABL Blank 22 299 13 120 16 370 26 430 19 503 14 300 10 667 12 455 23 353 12 691 Laboratories Replicates PML-RARa BCR1 **Blank** Blank BCR3 Blank Blank

tative assays for the most common fusion transcripts detectable in hematologic malignancies. However, because the ABI PRISM apparatus (ABI; Applied Biosystems) was the first available instrument for real-time PCR, most of the methods developed for the ABI PRISM use TaqMan probe chemistry (1–3). With the introduction of other real-time PCR instruments, such as the LightCycler (LC; Roche), other methods have been described (4–7). The instruments differ in several respects, including the light sources and the approach to acquisition of fluorescence data. Few reports have compared the results obtained with different types of real-time PCR instruments (8). To the best of our knowledge, no such multicenter studies with common calibrators and common methods have been reported.

In the present study we analyzed the results obtained with two of the more widely used instruments for real time PCR, i.e., the ABI and LC, for amplifying two rearrangements frequently detectable in human leukemia, the *BCR-ABL* and *PML-RARa* fusion genes. For *BCR-ABL* several quantitative methods have been established for both instruments (3–7), whereas for *PML-RARa* most of the quantitative methods have been developed for the ABI PRISM (1).

The quantification of *BCR-ABL* transcripts is clinically relevant for monitoring patients with chronic myeloid leukemia undergoing allogeneic hematopoietic stem cell transplantation (4, 9) or treatment with interferon-a or imatinib mesylate (9–11). For example, low numbers of *BCR-ABL* transcripts after 2 weeks of imatinib treatment predict a good response to imatinib after 4 weeks (9). With respect to *PML-RARa*, recent reports have shown that quantitative assessment of *PML-RARa* transcripts allowed efficient monitoring of minimal residual disease

1090 Technical Briefs

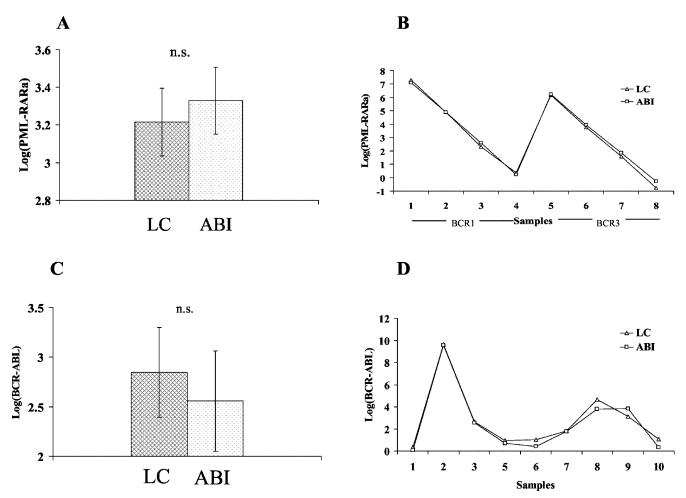


Fig. 1. Pooled means and profiles of means for the samples.

(A), pooled means of log(PML-RARa) for the LC and ABI. The error bars indicate 2 SD. (B), profiles of the means of the PML-RARa samples analyzed by each type of real-time PCR instrument. (C), pooled means of log(BCR-ABL) for the LC and ABI. The error bars indicate 2 SD. (D), profiles of the means of the BCR-ABL samples processed by each type of real-time PCR instrument. n.s., not significant.

(1) and assessment of the effects of the treatment given (12). Furthermore, patients who had transcription values above an empirical checkpoint after consolidation therapy had an increased risk of relapse (13).

Ten laboratories participated in the trial for *PML-RARa* analysis (6 using LC and 4 ABI), and 11 laboratories were involved in the *BCR-ABL* assay (7 using LC and 4 ABI; see the list of participating laboratories in the Data Supplement that accompanies the online version of this Technical Brief at http://www.clinchem.org/content/vol50/issue6/). In the trial for *PML-RARa*, each laboratory received 20 samples: 2 reagent blanks, 4 BCR1-positive, and 4 BCR3-positive cDNA samples in two replicates. In the trial for *BCR-ABL*, the laboratories received 10 samples: 1 blank and 9 patient cDNA samples (5 B3A2-positive and 4 B2A2-positive).

The laboratories also received calibrators prepared by cloning PCR products of samples from positive patients (B3A2 isoform for *BCR-ABL*, and BCR1 or BCR3 isoforms for *PML-RARa*) into CR® II-TOPO® vector (TOPOTM Cloning® Kit). For *PML-RARa*, two sets of calibrators were

prepared: one for BCR1 and the other for the BCR3 isoform. Calibrators were provided at the following concentrations: 2×10^5 , 2×10^4 , 2×10^2 , 2×10^1 , and 2 copies/ μ L. Samples and calibrators were shipped on dry ice by overnight courier and stored refrigerated until used. The calibrators were analyzed in duplicate and the samples in triplicate.

For *PML-RARa* quantification, the laboratories equipped with ABI used the reagents and protocol established by Gabert et al. (14, 15) for this instrument in the Europe Against Cancer Program (EAC Protocol April 2002). The method designed for the ABI PRISM was optimized in the LC by use of a final volume of 10 μ L, including 2 μ L of cDNA samples (unknowns) or 2 μ L of calibrators (for the calibration curve; see the Methods file in the online Data Supplement).

For the *BCR-ABL* rearrangement the laboratories equipped with ABI used the reagents and protocol designed by Gabert et al. (14, 15). The ABI method was also optimized for the LC as described (see the Methods file in the online Data Supplement).

The quantification of transcripts was carried out automatically with the software provided in each type of equipment (see the section on quantification in the Methods file in the online Data Supplement).

To compare the results among the laboratories or samples for each real-time instrument, we performed a multivariate ANOVA for laboratories and samples as described in the Statistics file in the online Data Supplement.

The efficiencies estimated from the slopes of the calibration curves for the *PML-RARa* BCR1 and BCR3 isoforms for the ABI and LC were very similar (Table 1 in the online Data Supplement). One false-positive result was detected in a BCR1 blank sample (Table 1).

All laboratories detected transcripts in the replicate of the BCR1-positive sample with the lowest number of copies, and three of the four ABI and two of the seven LC laboratories detected the replicate sample BCR3 with the lowest number of copies (Table 1). These results suggest that both instruments are capable of detecting 1–5 copies/ μ L of the *PML-RARa* isoforms.

We observed significant differences among global means of the PML-RARa results of the laboratories with LC or ABI (P = 0.000). However, the global means of all samples assessed with LC or ABI showed no statistical difference (Fig. 1A), as reflected in the profiles of the means of the samples processed by each real-time instrument (Fig. 1B).

We found a difference in the interaction reproducibility between the two instruments at the limits of statistical significance ($P \approx 0.05$; Table 2 in the online Data Supplement), which was attributable to the larger variance of the LC for this component.

The efficiencies estimated from the slope of the calibration curves for *BCR-ABL* were similar for the two instruments [mean (SD) 1.79 (0.04) for the LC and 1.84 (0.02) for the ABI; Table 1 in the online Data Supplement]. No false-positive results were reported for the blank controls (Table 1).

All participating laboratories except one using the LC were able to detect transcripts in the sample with the lowest amount of *BCR-ABL* transcripts (1–5 copies/ μ L; Table 1).

We observed significant differences among the global means of the laboratories using LC or ABI (P < 0.001). Conversely, we found no statistically significant differences between the ABI and LC instruments for the global means of pooled samples of the laboratories (Fig. 1C). In addition, the profiles of the means of log(BCR-ABL) obtained for each sample within the laboratories using an ABI or LC instrument were nearly identical (Fig. 1D).

None of the precision components differed between the ABI and LC (Table 2 in the online Data Supplement).

In summary, this multicenter study showed that the ABI and LC instruments performed similarly. As a multilaboratory trial, the results obtained can be expected to better transfer to the data reported in clinical trials than if the comparison were performed by a single laboratory. The study confirms the ability of the LC to use the

TaqMan technology (6, 16) as an alternative to the Hyb-Probes technology originally developed for this system (5, 17).

In this study, the main statistical differences were among the pooled means of the data. These individual differences among the laboratories with the same instrument could be attributable to variability in the stability of control samples or reagents, methodologic proficiency, or instrument maintenance.

The small difference in the interaction reproducibility ($P \approx 0.05$) for PML-RARa could reflect a difference in sensitivity of LC to the influence of noncontrolled effects.

In conclusion, despite differences in reagents in our study, the results for the LC and ABI instruments were equivalent with respect to the means and precision, suggesting that the choice of instrument has little to do with results when laboratories use the same methods and calibrators. Standardization of quantitative real-time PCR studies in a multiinstitutional context will require adoption of common methods and calibrators. The harmonization of the results should in turn allow better comparison of data obtained in different therapeutic trials.

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Size-Selective Extraction of Peptides from Urine for Mass Spectrometric Analysis, Glen L. Hortin, ^{1*} Bonnie Meilinger, ¹ and Steven K. Drake² (Departments of ¹ Laboratory Medicine and ² Critical Care Medicine, Warren Magnuson Clinical Center, NIH, Bethesda, MD; * address correspondence to this author at: Department of Laboratory Medicine, NIH, Bldg 10, Room 2C-407, Bethesda, MD 20892-1508; fax 301-402-1885, e-mail ghortin@mail.cc.nih. gov)

Protein excretion in urine has been suggested as an indicator of kidney disease since the time of Hippocrates. In the early 1800s, Bright further established approaches for studying proteinuria as a marker for kidney disease (1). As methods for quantitative and qualitative analysis have become more sophisticated, it has become possible to detect earlier stages of kidney disease and to differentiate different patterns of protein excretion (1–3). Quantitative immunoassays of selected urinary components such as α_1 -microglobulin, albumin, IgG, and α_2 -macroglobulin have been shown to be useful in characterizing the nature of proteinuria (4). Two-dimensional electrophoresis has provided a method for simultaneous analysis of numerous proteins in urine (5, 6). Recently, a new dimension has been added to analysis of urinary components by mass spectrometric techniques, which detect many small peptide components below the size resolution of electrophoresis (7, 8). The highly complex mixtures of small peptides in urine offer the potential for informationrich patterns for clinical diagnosis. Concentrations of urinary peptides serve not only as markers for kidney function but also as markers of other systemic physiologic processes. As examples, immunoassays for specific peptides provide measures of thrombosis and fibrinolysis (9, 10) and endocrine function (11).

In the present study, we sought to identify a simple method to prepare urine specimens for the analysis of small peptide components. Sample preparation represents one of the major challenges for analysis of peptide components in urine specimens by mass spectrometry. Ideally, sample preparation needs to accomplish three tasks: (a) concentration of relatively dilute peptide components; (b) removal of salts that suppress peptide ionization in mass spectrometry; and (c) depletion of albumin and other high-molecular-weight components that comprise most of the total protein mass in urine. Standard methods that have been applied for protein concentration—centrifugal ultrafiltration, acetone precipitation, acid precipitation, dye precipitation, ultracentrifugation, and lyophilization-generally have drawbacks of poor peptide recovery, poorly soluble pellets, or failure to remove salts (6). We examined solid-phase extraction of urinary peptides, using a polymeric sorbent with a pore size that should exclude albumin and other proteins of similar or greater size.

Urine specimens were processed in 6-mL cartridges containing 500 mg of StrataTM-X polymeric sorbent (Phenomenex) on a vacuum manifold. Pore size of the sorbent was specified by the manufacturer to be 91 Å, yielding a predicted size exclusion limit of ~20 000 Da. Cartridges were primed with 4 mL of methanol followed by 4 mL of 5 g/L acetic acid before addition of urine specimens, which had been acidified with acetic acid during collection to a pH of 4-5. After extraction of urine, cartridges were washed with 8 mL of 5 g/L acetic acid, and peptides were eluted with 3-mL steps of increasing acetonitrile concentration or with 600 mL/L acetonitrile-5 g/L acetic acid. Measurements of total protein and albumin to determine the amounts of proteins eluted from the cartridges were performed by standard methods (pyrogallol red and immunoturbidimetry, respectively) on a LX-20 analyzer (Beckman-Coulter). C-Peptide was measured by competitive immunoassay with an Immulite 2000 (Diagnostics Products Corp.). Eluates from extraction cartridges were analyzed either after evaporation under nitrogen to \sim 2 mL or directly.

Matrix-assisted laser desorption/ionization time-of-flight (MALDI TOF) mass spectrometry was performed with an Ultraflex TOF mass spectrometer (Bruker Daltonics) in a linear positive-ion mode. Specimens were applied manually to 384-position target plates as 1-μL aliquots between layers of matrix applied as 1-μL aliquots of 10 g/L sinapinic acid in 750 mL/L acetonitrile–250 mL/L water containing 10 g/L acetic acid. Data were summed for 300 laser pulses collected from 10 positions. Measurements of mass/charge (*m*/*z*) were by external calibration. Calibrators and sinapinic acid were purchased from Bruker Daltonics.

Solid-phase extraction of highly proteinuric urine (Table 1) served as good example of the size selectivity and binding capacity of the extraction cartridge. We loaded 10-mL aliquots of urine successively on a single cartridge and analyzed the eluates. The albumin concentrations of flow throughs were approximately the same as the initial